

Correlations in Complex Systems

Significant Memory Effects Typically Cause Long Time Correlations in Complex Systems

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Glossary

Correlation A correlation describes the degree of relationship between two or more variables. The correlations are viewed due to the impact of random factors and can be characterized by the methods of probability theory.

Correlation function The correlation function (abbreviated, as CF) represents the quantitative measure for the compact description of the wide classes of correlation in the complex systems (CS). The correlation function of two variables in statistical mechanics provides a measure of the mutual order existing between them. It quantifies the way random variables at different positions are correlated. For example in a spin system, it is the thermal average of the scalar product of the spins at two lattice points over all possible orderings.

Memory effects in stochastic processes through correlations Memory effects (abbreviated, as ME) appear at a more detailed level of statistical description of correlation in the hierarchical manner. ME reflect the complicated or hidden character of creation, the propagation and the decay of correlation. ME are produced

by inherent interactions and statistical after-effects in CS. For the statistical systems ME are induced by contracted description of the evolution of the dynamic variables of a CS.

Memory functions Memory functions describe mutual interrelations between the rates of change of random variables on different levels of the statistical description. The role of memory has its roots in the natural sciences since 1906 when the famous Russian mathematician Markov wrote his first paper in the theory of Markov Random Processes. The theory is based on the notion of the instant loss of memory from the prehistory (memoryless property) of random processes.

Information measures of statistical memory in complex systems From the physical point of view time scales of correlation and memory cannot be treated as arbitrary. Therefore, one can introduce some statistical quantifiers for the quantitative comparison of these time scales. They are dimensionless and possess the statistical spectra on the different levels of the statistical description.

Definition of the Subject

As commonly used in probability theory and statistics, a correlation (also so called correlation coefficient), measures the strength and direction of a linear relationship between two random variables. In a more general sense, a correlation or co-relation reflects the deviation of two (or more) variables from mutual independence, although correlation does not imply causation. In this broad sense there are some quantifiers which measures the degree of correlation, suited to the nature of data. Increasing attention has been paid recently to the study of statistical memory effects in random processes that originate from nature by means of non-equilibrium statistical physics. The role of memory has its roots in natural sciences since 1906 when the famous Russian mathematician Markov wrote his first paper on the theory of Markov Random Processes (MRP) [1]. His theory is based on the notion of an instant loss of memory from the prehistory (memoryless property) of random processes. In contrast, there are an abundance of physical phenomena and processes which can be characterized by statistical memory effects: kinetic and relaxation processes in gases [2] and plasma [3], condensed matter physics (liquids [4], solids [5], and superconductivity [6]) astrophysics [7], nuclear physics [8], quantum [9] and classical [9] physics, to name only a few. At present, we have a whole toolbox available of statistical methods which can be efficiently used for the analysis of the memory effects occurring in diverse physical systems. Typical such

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schemes are Zwanzig–Mori’s kinetic equations [10,11], generalized master equations and corresponding statistical quantifiers [12,13,14,15,16,17,18], Lee’s recurrence relation method [19,20,21,22,23], the generalized Langevin equation (GLE) [24,25,26,27,28,29], etc.

Here we shall demonstrate that the presence of statistical memory effects is of salient importance for the functioning of the diverse natural complex systems. Particularly, it can imply that the presence of large memory times scales in the stochastic dynamics of discrete time series can characterize catastrophic (or pathological for live systems) violation of salutary dynamic states of CS. As an example, we will demonstrate here that the emergence of strong memory time scales in the chaotic behavior of complex systems (CS) is accompanied by the likely initiation and the existence of catastrophes and crises (Earthquakes, financial crises, cardiac and brain attack, etc.) in many CS and especially by the existence of pathological states (diseases and illness) in living systems.

Introduction

A common definition [30] of a correlation measure $\rho(X, Y)$ between two random variables X and Y with the mean values $E(X)$ and $E(Y)$, and fluctuations $\delta X = X - E(X)$ and $\delta Y = Y - E(Y)$, dispersions $\sigma_X^2 = E(\delta X^2) = E(X^2) - E(X)^2$ and $\sigma_Y^2 = E(\delta Y^2) = E(Y^2) - E(Y)^2$ is defined by:

$$\rho(X, Y) = \frac{E(\delta X \delta Y)}{\sigma_X \sigma_Y},$$

where E is the expected value of the variable. Therefore we can write

$$\rho(X, Y) = \frac{[E(XY) - E(X)E(Y)]}{(E(X^2) - E(X)^2)^{1/2} (E(Y^2) - E(Y)^2)^{1/2}}.$$

Here, a correlation can be defined only if both of the dispersions are finite and both of them are nonzero. Due to the Cauchy–Schwarz inequality, a correlation cannot exceed 1 in absolute value. Consequently, a correlation assumes its maximum at 1 in the case of an increasing linear relationship, or -1 in the case of a decreasing linear relationship, and some value in between in all other cases, indicating the degree of linear dependence between the variables. The closer the coefficient is either to -1 or 1 , the stronger is the correlation between the variables. If the variables are independent then the correlation equals 0, but the converse is not true because the correlation coefficient detects only linear dependencies between two variables.

Since the absolute value of the sample correlation must be less than or equal to 1 the simple formula conveniently suggests a single-pass algorithm for calculating sample correlations. The square of the sample correlation coefficient, which is also known as the coefficient of determination, is the fraction of the variance in σ_x that is accounted for by a linear fit of x_i to σ_y . This is written

$$R_{xy}^2 = 1 - \frac{\sigma_{y|x}^2}{\sigma_y^2},$$

where $\sigma_{y|x}^2$ denotes the square of the error of a linear regression of x_i on y_i in the equation $y = a + bx$,

$$\sigma_{y|x}^2 = \frac{1}{n} \sum_{i=1}^n (y_i - a - bx_i)^2$$

and σ_y^2 denotes just the dispersion of y .

Note that since the sample correlation coefficient is symmetric in x_i and y_i , we will obtain the same value for a fit to y_i :

$$R_{xy}^2 = 1 - \frac{\sigma_{x|y}^2}{\sigma_x^2}.$$

This equation also gives an intuitive idea of the correlation coefficient for random (vector) variables of higher dimension. Just as the above described sample correlation coefficient is the fraction of variance accounted for by the fit of a 1-dimensional linear submanifold to a set of 2-dimensional vectors (x_i, y_i) , so we can define a correlation coefficient for a fit of an m -dimensional linear submanifold to a set of n -dimensional vectors. For example, if we fit a plane $z = a + bx + cy$ to a set of data (x_i, y_i, z_i) then the correlation coefficient of z to x and y is

$$R^2 = 1 - \frac{\sigma_{z|xy}^2}{\sigma_z^2}.$$

Correlation and Memory in Discrete Non-Markov Stochastic Processes

Here we present a non-Markov approach [31,32] for the study of long-time correlations in chaotic long-time dynamics of CS. For example, let the variable x_i be defined as the R-R interval or the time distance between nearest, so called R peaks occurring in a human electrocardiogram (ECG). The generalization will consist in taking into account non-stationarity of stochastic processes and its further applications to the analysis of the heart-rate variability.

We should bear in mind, that one of the key moments of the spectral approach in the analysis of stochastic processes consists in the use of normalized time correlation function (TCF)

$$a_0(t) = \frac{\langle\langle \mathbf{A}(T) \mathbf{A}(T+t) \rangle\rangle}{\langle \mathbf{A}(T)^2 \rangle}. \quad (1)$$

Here the time T indicates the beginning of a time serial, $\mathbf{A}(t)$ is a state vector of a complex system as defined below in Eq. (5) at t , $|\mathbf{A}(t)|$ is the length of vector $\mathbf{A}(t)$, the double angular brackets indicate a scalar product of vectors and an ensemble averaging. The ensemble averaging is, of course needed in Eq. (1) when correlation and other characteristic functions are constructed. The average and scalar product becomes equivalent when a vector is composed of elements from a discrete-time sampling, as done later. Here a continuous formalism is discussed for convenience. However further, since Sect. "Correlation and Memory in Discrete Non-Markov Stochastic Processes" we shall consider only a case of discrete processes.

The above-stated designation is true only for stationary systems. In a non-stationary case Eq. (1) is not true and should be changed. The concept of TCF can be generalized in case of discrete non-stationary sequence of signals. For this purpose the standard definition of the correlation coefficient in probability theory for the two random signals X and Y must be taken into account

$$\rho = \frac{\langle\langle \mathbf{X}\mathbf{Y} \rangle\rangle}{\sigma_X \sigma_Y}, \quad \sigma_X = \langle|\mathbf{X}|\rangle, \quad \sigma_Y = \langle|\mathbf{Y}|\rangle. \quad (2)$$

In Eq. (2) the multi-component vectors \mathbf{X} , \mathbf{Y} are determined by fluctuations of signals x and y accordingly, σ_X^2, σ_Y^2 represent the dispersions of signals \mathbf{x} and \mathbf{y} , and values $|\mathbf{X}|, |\mathbf{Y}|$ represent the lengths of vectors \mathbf{X} , \mathbf{Y} , correspondingly. Therefore, the function

$$a(T, t) = \frac{\langle\langle \mathbf{A}(T) \mathbf{A}(T+t) \rangle\rangle}{\langle|\mathbf{A}(T)|\rangle \langle|\mathbf{A}(T+t)|\rangle} \quad (3)$$

can serve as the generalization of the concept of TCF (1) for non-stationary processes $\mathbf{A}(T+t)$. The non-stationary TCF (3) obeys the conditions of the normalization and attenuation of correlation

$$a(T, 0) = 1, \quad \lim_{t \rightarrow \infty} a(T, t) = 0.$$

Let us note, that in a real CS the second limit, typically, is not carried out due possible occurrence nonergodicity (meaning that a time average does not equal its ensemble average). According to the Eqs. (1) and (3) for the quantitative description of non-stationarity it is convenient to

introduce a function of non-stationarity

$$\gamma(T, t) = \frac{\langle|\mathbf{A}(T+t)|\rangle}{\langle|\mathbf{A}(T)|\rangle} = \left\{ \frac{\sigma^2(T+t)}{\sigma^2(T)} \right\}^{1/2}. \quad (4)$$

One can see that this function equals the ratio of the lengths of vectors of final and initial states. In case of stationary process the dispersion does not vary with the time (or its variation is very weak). Therefore the following relations

$$\sigma(T+t) = \sigma(T), \quad \gamma(T, t) = 1 \quad (5)$$

hold true for the stationary process.

Due to the condition (5) the following function

$$\Gamma(T, t) = 1 - \gamma(T, t) \quad (6)$$

is suitable in providing a dynamic parameter of non-stationarity. This dynamic parameter can serve as a quantitative measure of non-stationarity of the process under investigation. According to Eqs. (4)–(6) it is reasonable to suggest the existence of three different elementary classes of non-stationarity

$$|\Gamma(T, t)| = |1 - \gamma(T, t)| = \begin{cases} \ll 1, & \text{weak non-stationarity} \\ \sim 1, & \text{intermediate non-stationarity} \\ \gg 1, & \text{strong non-stationarity} \end{cases}. \quad (7)$$

The existence of dynamic parameter of non-stationarity makes it possible to determine, on-principle, the type of non-stationarity of the underlying process and to find its spectral characteristics from the experimental data base. We intend to use Eqs. (4), (6), (7) for the quantitative description of effects of non-stationarity in the investigated temporary series of R-R intervals of human ECG's for healthy people and patients after myocardial infarction (MI).

Statistical Theory of Non-Stationary Discrete Non-Markov Processes in Complex Systems **TS2**

Here we shall extend the original results of the statistical theory of discrete non-Markov processes in complex systems, developed recently in [31], for the case of non-stationary processes. The theory [31] is developed on the basis of first principles and represents a discrete finite-difference analogy for complex systems of well known Zwanzig–Mori's kinetic equations [10,11,12,13,14,15,16,17,18] used in the statistical physics of condensed matter.

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We examine a discrete stochastic process $X(T + t)$, where $t = m\tau$

$$X = \{x(T), x(T + \tau), x(T + 2\tau), \dots, x(T + k\tau), \dots, x(T + (N - 1)\tau)\}, \quad (8)$$

where T is the beginning of the time and τ is a discretization time. The normalized time correlation function (TCF)

$$a(t) = \frac{1}{(N - m)\sigma^2} \sum_{j=0}^{N-1-m} \delta x(T + j\tau) \delta x(T + (j + m)\tau) \quad (9)$$

yields a convenient measure to analyze the dynamic properties of complex systems. Herein, we used the variance σ^2 , the fluctuation $\delta x(T + j\tau)$, which in terms of the the mean value $\langle x \rangle$ reads:

$$\delta x_j = \delta x(T + j\tau) = x(T + j\tau) - \langle x \rangle, \quad (10)$$

$$\sigma^2 = \frac{1}{(N - m)} \sum_{j=0}^{N-1-m} \{\delta x(T + j\tau)\}^2,$$

$$\langle x \rangle = \frac{1}{(N - m)} \sum_{j=0}^{N-1-m} x(T + j\tau). \quad (11)$$

The discrete time t is given as $t = m\tau$.

In general, the mean value, the variance and TCF in (9), (10) and (11) is dependent on the numbers m and N . All indicated values cease to depend on numbers m and N for stationary processes when $m \ll N$. The definition of TCF in Eq. (9) is true only for stationary processes.

Next, we shall try to take into account this important dependence. With this purpose we shall form two k -dimensional vectors of state by the process (8):

$$\mathbf{A}_k^0 = (\delta x_0, \delta x_1, \delta x_2, \dots, \delta x_{k-1}), \quad (12)$$

$$\mathbf{A}_{m+k}^m = (\delta x_m, \delta x_{m+1}, \delta x_{m+2}, \dots, \delta x_{m+k-1}).$$

When a vector of a state is composed of elements from a discrete-time sampling, the average and scalar product in Eq. (1) become equivalent. In an Euclidean space of vectors of state (12) TCF $a(t)$

$$a(t) = \frac{\langle \mathbf{A}_{N-1-m}^0 \mathbf{A}_{N-1}^m \rangle}{(N - m)\{\sigma(N - m)\}^2} = \frac{\langle \mathbf{A}_{N-1-m}^0 \mathbf{A}_{N-1}^m \rangle}{|\mathbf{A}_{N-1-m}^0|^2} \quad (13)$$

describes the correlation of two different states of the system ($t = m\tau$). Here the brackets $\langle \dots \rangle$ indicate the scalar product of the two vectors. The dimension dependence of the corresponding vectors is also taken into account

in the variance $\sigma = \sigma(N - m)$. As a matter of fact TCF $a(t) = \cos \vartheta$, where ϑ is the angle between the two vectors from Eq. (12). Let's introduce a unit vector of dimension $(N - m)$ in the following way:

$$\mathbf{n} = \frac{\mathbf{A}_{N-1-m}^0}{\sqrt{(N - m)\sigma^2}}. \quad (14)$$

Then, the TCF $a(t)$ (9) is given by

$$a(t) = \langle \mathbf{n}(0) \mathbf{n}(t) \rangle. \quad (15)$$

From the above discussion it is evident that Eqs. (13)–(15) are true for the stationary processes only. In case of non-stationary processes it is necessary to redefine TCF, taking into account the non-stationarity in the variance σ^2 in a line with Eqs.(2)–(7). For this purpose we shall redefine a unit vector of the final state as following

$$\mathbf{n}(t) = \frac{\mathbf{A}_{N-1}^m(t)}{|\mathbf{A}_{N-1}^m(t)|}. \quad (16)$$

For non-stationary processes it is convenient to write the TCF as the scalar product of the two unit vectors of the initial and final states

$$a(t) = \langle \mathbf{n}(0) \mathbf{n}(t) \rangle = \frac{\langle \mathbf{A}_{N-1-m}^0(0) \mathbf{A}_{N-1}^m(t) \rangle}{|\mathbf{A}_{N-1-m}^0(0)| |\mathbf{A}_{N-1}^m(t)|}. \quad (17)$$

Now we shall turn to the the dynamics of a non-stationary stochastic process. The equation of motion of a the random process x_j can be written in a finite-difference form for $0 \leq j \leq N - 1$ [15] in the following way

$$\frac{dx_j}{dt} \Rightarrow \frac{\Delta \delta x_j}{\Delta t} = \frac{\delta x_j(t + \tau) - \delta x_j(t)}{\tau}. \quad (18)$$

Then it is convenient to define the discrete evolution single step operator \hat{U} as following:

$$x(T + (j + 1)\tau) = \hat{U}(T + (j + 1)\tau, T + j\tau) x(T + j\tau). \quad (19)$$

In the case of stationary process we can rewrite the equation of motion (18) in a more simple form

$$\frac{\Delta \delta x_j}{\Delta t} = \tau^{-1} \{\hat{U}(\tau) - 1\} \delta x_j. \quad (20)$$

The invariance of the mean value $\langle x \rangle$ is taken into account in an Eq. (20)

$$\langle x \rangle = \hat{U}(\tau) \langle x \rangle, \quad \{\hat{U}(\tau) - 1\} \langle x \rangle = 0. \quad (21)$$

In case of a non-stationary process it is necessary to turn to the equation of motion for vector of the final state $\mathbf{A}_{m+k}^m(t)$ ($k = N - 1 - m$)

$$\frac{\Delta \mathbf{A}_{m+k}^m(t)}{\Delta t} = i \hat{L}(t, \tau) \mathbf{A}_{m+k}^m(t), \quad (22)$$

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326 where Liouville's quasioperator is

$$327 \quad \hat{L}(t, \tau) = (i\tau)^{-1} \{ \hat{U}(t + \tau, t) - 1 \}. \quad (23)$$

328 It is well known that, in general, a stochastic trajec-
329 tory does not obey a linear equation, so the general evolu-
330 tion operator and Liouville's quasioperator should prob-
331 ably be non-linear. Furthermore, in statistical physics the
332 Liouville's operator acts upon the probability densities of
333 dynamical variables, as well upon the variables itself like
334 in Mori's paper [12]. The evolution of the density would
335 be indeed linear. But Mori used the Liouville operator
336 in the quantum equation of motion in [12]. In line with
337 Mori [12] Eqs. (20), (22) can be considered as formal and
338 exact equations of the motion of a complex system.

339 Thus, due to the Eqs. (17), (22) and (23) we may take
340 into account the non-stationarity of the stochastic process.
341 Towards this goal let's introduce the linear projection op-
342 erator in Euclidean space of the state vectors

$$343 \quad \Pi \mathbf{A}(t) = \frac{\mathbf{A}(0) \langle \mathbf{A}(0) | \mathbf{A}(t) \rangle}{|\mathbf{A}(0)|^2}, \quad \Pi = \frac{\mathbf{A}(0) \langle \mathbf{A}(0) |}{\langle \mathbf{A}(0) | \mathbf{A}(0) \rangle}, \quad (24)$$

344 where angular brackets in numerator present the bound-
345 aries of action for the scalar product. TS4

346 For the analyzing the dynamics TS4 of the stochastic
347 process $\mathbf{A}(t)$ the vector $\mathbf{A}_k^0(0)$ from (12) can be considered
348 as a vector of the initial state $\mathbf{A}(0)$, and vector $\mathbf{A}_{m+k}^m(t)$
349 from (12) at value $m+k = N-1$ can be considered as
350 the vector of the final state $\mathbf{A}(t)$.

351 It is necessary to note that the projection operator (24)
352 has the required property of idem-potency $\Pi^2 = \Pi$. The
353 presence of operator Π allows one to introduce the mutu-
354 ally supplementary projection operator P :

$$355 \quad P = 1 - \Pi, \quad P^2 = P, \quad \Pi P = P \Pi = 0. \quad (25)$$

356 It is necessary to remark, that both projectors Π and P are
357 linear and can be recorded for the fulfillment of operations
358 in the particular Euclidean space. Due to the property (17)
359 and Eq. (4) it is easy to obtain the required TCF:

$$360 \quad \begin{aligned} \Pi \mathbf{A}(t) &= \Pi \mathbf{A}_{m+k}^m(t) \\ &= \mathbf{A}_k^0(0) \langle \mathbf{n}_k^0(0) | \mathbf{n}_{k+m}^m(t) \rangle \gamma_1(t) \\ &= \mathbf{A}_k^0(0) a(t) \gamma_1(t), \end{aligned} \quad (26)$$

$$361 \quad \gamma_1(t) = \frac{|\mathbf{A}_{m+k}^m(t)|}{|\mathbf{A}_m^0(0)|}.$$

362 Therefore the projector Π generates a unit vector along
363 the vector of the final state $\mathbf{A}(t)$ and makes its projection
364 onto the initial state vector $\mathbf{A}(0)$.

365 The existence of a pair of two mutually supplementary
projection operators Π and P allows one to carry out the

366 splitting of Euclidean space of vectors $\mathbf{A}(\mathbf{A}(0), \mathbf{A}(t) \in A)$
367 into a straight sum of two mutually supplementary sub-
368 spaces in the following way

$$A = A' + A'', \quad A' = \Pi A, \quad A'' = P A. \quad (27)$$

370 Substituting Eq. (27) in Eq. (23) we find Liouville's
371 quasioperator \hat{L} in a matrix form

$$372 \quad \hat{L} = \hat{L}_{11} + \hat{L}_{12} + \hat{L}_{21} + \hat{L}_{22}, \quad (28)$$

373 where the matrix elements are introduced

$$374 \quad \begin{aligned} \hat{L}_{11} &= \Pi \hat{L} \Pi, \quad \hat{L}_{12} = \Pi \hat{L} P, \\ \hat{L}_{21} &= P \hat{L} \Pi, \quad \hat{L}_{22} = P \hat{L} P. \end{aligned} \quad (29)$$

375 The Euclidean space of values of Liouville's quasiop-
376 erator $W = \hat{L} A$ will be generated by the vectors \mathbf{W} of di-
377 mension $k-1$

$$378 \quad \begin{aligned} (\mathbf{W}(0) \in W, \mathbf{W}(t) \in W) \\ W = W' + W'', \quad W' = \Pi W, \quad W'' = P W. \end{aligned} \quad (30)$$

379 Matrix elements \hat{L}_{ij} of the contracted description

$$380 \quad \hat{L} = \begin{pmatrix} \hat{L}_{11} & \hat{L}_{12} \\ \hat{L}_{21} & \hat{L}_{22} \end{pmatrix} \quad (31)$$

381 are acting in the following way:

$$382 \quad \begin{aligned} \hat{L}_{11} &- \text{from a subspace } A' \text{ to subspace } W', \\ \hat{L}_{12} &- \text{from } A'' \text{ to } W', \\ \hat{L}_{21} &- \text{from } W' \text{ to } W'' \text{ and} \\ \hat{L}_{22} &- \text{from } A'' \text{ to } W''. \end{aligned}$$

383 The projection operators Π and P provide the con-
384 tracted description of the stochastic process. Splitting the
385 dynamic Eq. (22) into two equations in the two mutually
386 supplementary Euclidean subspaces (see, for example [11]
387 TS5), we find

$$388 \quad \frac{\Delta \mathbf{A}'(t)}{\Delta t} = i \hat{L}_{11} \mathbf{A}'(t) + i \hat{L}_{12} \mathbf{A}''(t), \quad (32)$$

$$389 \quad \frac{\Delta \mathbf{A}''(t)}{\Delta t} = i \hat{L}_{21} \mathbf{A}'(t) + i \hat{L}_{22} \mathbf{A}''(t). \quad (33)$$

390 Following [31,32] it is necessary to eliminate first
391 the irrelevant part $\mathbf{A}''(t)$ in order to simplify Liouville's
392 Eq. (22) and then to write a closed equation for relevant
393 part $\mathbf{A}'(t)$. According to [32] that can be achieved by a se-
394 ries of successive steps (for example, see Eqs. (32)–(36)

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TS5 Please check if this reference is correct or clarify which reference "10b" is.

in [32]). First a solution to Eq. (33) for the first step can be obtained in a form

$$\begin{aligned} \frac{\Delta \mathbf{A}''(t)}{\Delta t} &= \frac{\mathbf{A}''(t + \tau) - \mathbf{A}''(t)}{\tau} \\ &= i\hat{L}_{21} \mathbf{A}'(t) + i\hat{L}_{22} \mathbf{A}''(t), \\ \mathbf{A}''(t + \tau) &= \mathbf{A}''(t) + i\tau \hat{L}_{21} \mathbf{A}'(t) + i\tau \hat{L}_{22} \mathbf{A}''(t) \\ &= \{1 + i\tau \hat{L}_{22}\} \mathbf{A}''(t) + i\tau \hat{L}_{21} \mathbf{A}'(t) \\ &= U_{22}(t + \tau, t) \mathbf{A}''(t) + i\tau \hat{L}_{21}(t + \tau, t) \mathbf{A}'(t). \end{aligned} \quad (34)$$

We next can derive a finite-difference kinetic equation of a non-Markov type for TCF $a(t = m\tau)$

$$\frac{\Delta a(t)}{\Delta t} = \lambda_1 a(t) - \tau \Lambda_1 \sum_{j=0}^{m-1} M_1(t - j\tau) a(j\tau). \quad (35)$$

Here, λ_1 is a eigenvalue, Λ_1 is a relaxation parameter of Liouville's quasioperator \hat{L}

$$\begin{aligned} \lambda_1 &= i \frac{\langle \mathbf{A}_k^0(0) \hat{L} \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2}, \\ \Lambda_1 &= \frac{\langle \mathbf{A}_k^0(0) \hat{L}_{12} \hat{L}_{21} \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2} = \frac{\langle \mathbf{A}_k^0(0) \hat{L}^2 \mathbf{A}_k^0(0) \rangle}{|\mathbf{A}_k^0(0)|^2}, \end{aligned} \quad (36)$$

The angular brackets indicate here a scalar product of new state vectors. Function $M_1(t - j\tau)$ on the right side of Eq. (35) represents a modified memory function (MF) of the first order

$$M_1(t - j\tau) = \frac{\gamma_1(t - j\tau)}{\gamma_1(t)} m_1(t - j\tau). \quad (37)$$

For stationary processes the function $\gamma_1(t)$ approaches unity. Then the memory functions $M_1(t)$ and $m_1(t)$ coincide with each other. The latter equation is the first kinetic finite-difference equation for TCF. It is remarkable, that the non-Markovity, discretization and non-stationarity of stochastic process can be considered explicitly. Due to the presence of non-stationarity both in TCF and in the first memory function this equation generalizes our results recently obtained in [31].

Following the projection technique described above, we arrive at a chain of connected kinetic finite-difference equations of a non-Markov type for the normalized short memory functions $m_n(t)$ in Euclidean space of state vec-

tors of dimension $(k - n)$ ($t = m\tau, n \geq 1$)

$$\begin{aligned} \frac{\Delta m_n(t)}{\Delta t} &= \lambda_{n+1} m_n(t) - \tau \Lambda_{n+1} \\ &\times \sum_{j=0}^{m-1} m_{n+1}(j\tau) m_n(t - j\tau) \\ &\times \left\{ \frac{\gamma_{n+1}(j\tau) \gamma_{n+1}(t - j\tau)}{\gamma_n(t)} \right\}, \end{aligned} \quad (38)$$

$$\begin{aligned} m_{n+1}(t) &= \frac{\langle \mathbf{W}_{n+1}(0) \mathbf{W}_{n+1}(t) \rangle}{|\mathbf{W}_{n+1}(0)| |\mathbf{W}_{n+1}(t)|}, \\ \gamma_n(j\tau) &= \left\{ \frac{|\mathbf{W}_n(j\tau)|}{|\mathbf{W}_n(0)|} \right\}. \end{aligned} \quad (39)$$

Here, $\gamma_n(j\tau)$ is the n th order of the non-stationarity function.

The set of all memory functions $m_1(t), m_2(t), m_3(t), \dots$ allows one to describe non-Markov processes and statistical memory effects in the considered non-stationary system. For the particular case we obtain a more simple form for the set of equations for the first three short memory functions, namely ($t = m\tau$):

$$\begin{aligned} \frac{\Delta a(t)}{\Delta t} &= -\tau \Lambda_1 \sum_{j=0}^{m-1} m_1(j\tau) \left\{ \frac{\gamma_1(j\tau) \gamma_1(t - j\tau)}{\gamma_1(t)} \right\} \\ &\times a(t - j\tau) + \lambda_1 a(t), \\ \frac{\Delta m_1(t)}{\Delta t} &= -\tau \Lambda_2 \sum_{j=0}^{m-1} m_2(j\tau) \left\{ \frac{\gamma_2(j\tau) \gamma_2(t - j\tau)}{\gamma_2(t)} \right\} \\ &\times m_1(t - j\tau) + \lambda_2 m_1(t), \\ \frac{\Delta m_2(t)}{\Delta t} &= -\tau \Lambda_3 \sum_{j=0}^{m-1} m_3(j\tau) \left\{ \frac{\gamma_3(j\tau) \gamma_3(t - j\tau)}{\gamma_3(t)} \right\} \\ &\times m_2(t - j\tau) + \lambda_3 m_2(t). \end{aligned} \quad (40)$$

Here the relaxation parameters Λ_1, Λ_2 and Λ_3 have already been determined and the non-stationarity functions $\gamma_n(t)$ have been introduced earlier. By analogy with Eq. (6) we can introduce a set of dynamic parameters of non-stationarity (PNS) for the arbitrary n th relaxation level

$$\Gamma_n(T, t) = 1 - \gamma_n(t) = 1 - \gamma_n(T, t). \quad (41)$$

The whole set of values of dynamic PNS $\gamma_n(t)$ determines the broad spectrum of non-stationarity effects of the considered process.

The obtained equations are similar to the well known Zwanzig–Mori's kinetic equations [10,11,12,13,14,15,16,17,18] used in non-equilibrium statistical physics of condensed matters. Let us point out three essential distinctions of our Eqs. (40) from the results in [10,11,12]. In

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448 Zwanzig–Mori’s theory the key moment in the analysis of
 449 considered physical systems is the presence of a Hamil-
 450 tonian and an operation of a statistical averaging carried
 451 out with the help of quantum density operator or classic
 452 Gibbs distribution function [33]. In our examined case,
 453 both the Hamiltonian and the distribution function are ab-
 454 sent. There are exact classic or quantum equations of mo-
 455 tion in physics; so Liouville’s equation and Liouville’s op-
 456 erator are useful in many applications. The motion of indi-
 457 vidual particles and whole statistic system is described by
 458 variables varying in continuous time. Therefore, for phys-
 459 ical systems it is possible to use effectively the methods of
 460 integro-differential calculus, based on the mathematically
 461 accustomed (but from the physical point of view difficult
 462 for understanding) representation of infinitesimal varia-
 463 tions of values of coordinates and time. By nature, the
 464 monitored time evolution of most complex systems is dis-
 465 crete. As well known, discretization is inherent in a wide
 466 variety both of classical and quantum complex systems.
 467 This forces us to abandon the concept of an infinite small
 468 values and continuity and instead turn to discrete-differ-
 469 ence schemes. And, at last, the third feature is connected
 470 with incorporating the issue of non-stationary processes
 471 into our theory. The Zwanzig–Mori theory is typically ap-
 472 plied only for stationary processes. Due to the introduc-
 473 tion of normalized vectors of states and the use of the ap-
 474 propriate projection technique [13] our theory allows to
 475 take into account non-stationary processes as well. The lat-
 476 ter ones can be described by the non-Markov kinetic equa-
 477 tions together with the introduction of the set of non-sta-
 478 tionarity functions.

479 The non-stationary theory [32] put forward here dif-
 480 fers from the stationary case [31]. The external structure of
 481 the kinetic equations remains invariant; they represent the
 482 kinetic equations with memory. However, the functions
 483 and the parameters, which are included in these equa-
 484 tions, appreciably differ from each other. As we already
 485 remarked above, non-stationarity effects enter both, in the
 486 functions $\gamma_n(t)$ and in spectral and kinetic parameters.

487 **Correlation and Memory in Discrete Non-Markov**
 488 **Stochastic Processes Generated by Random Events**

489 Here we shall find a chain of the kinetic interconnected
 490 finite-difference equations for a discrete correlation func-
 491 tion $a(n)$ and memory functions $M_s(n)$ in the linear scale
 492 of events $E = \{\xi_1, \xi_2, \xi_3, \dots, \xi_N\}$.

The Basic Assumptions and Concepts of the Theory
of Discrete Non-Markov Stochastic Processes
of the Events Correlations

As an example we shall consider the time variations of the
 total X-ray flux of an astrophysical object at a succession
 of events:

$$E = \{\xi_1, \xi_2, \xi_3, \dots, \xi_k, \dots, \xi_N\}, \quad (42)$$

where ξ_i is an event, which occurs at time instant t_i , where
 $i = 1, \dots, N$ counts the event number.

The average value $\langle E \rangle$, fluctuations $\delta\xi$ and disper-
 sion σ^2 for the set of N events are obtained as:

$$\langle E \rangle = \frac{1}{N} \sum_{i=1}^N \xi_i, \delta\xi_i = \xi_i - \langle E \rangle, \quad (43)$$

$$\sigma^2 = \frac{1}{N} \sum_{i=1}^N \delta\xi_i^2 = \frac{1}{N} \sum_{i=1}^N \{\xi_i - \langle E \rangle\}^2.$$

According to [35,36,37,38], for the description of the
 dynamical properties of the studied system we introduce
 the correlation dependence of the discrete set of events
 (see Eq. (42)) using the CF:

$$a(n) = \frac{1}{(N - m) \sigma^2} \sum_{i=1}^{N-m} \delta\xi_i \delta\xi_{i+m}. \quad (44)$$

Here $n = m\Delta n$, $\Delta n = 1$ is the discretization step. The
 function $a(n)$, which emerges in this way, is the “event”
 correlation function (ECF). The normalized ECF must
 obey the conditions of normalization and of the attenu-
 ation of correlation, i. e.: $\lim_{n \rightarrow 1} a(n) = 1$, $\lim_{n \rightarrow \infty} a(n)$
 $= 0$. We remark, however, that the second condition for
 the case the physical complex systems is typically not ob-
 served (at $N \gg 0$). It is necessary to note that in [18] the
 correlation function for the aftershock events has been in-
 troduced:

$$C(n + n_W, n_W) = \frac{[\langle t_{n+n_W} t_{n_W} \rangle - \langle t_{n+n_W} \rangle \langle t_{n_W} \rangle]}{(\sigma_{n+n_W}^2 \sigma_{n_W}^2)^{1/2}},$$

where the averages and the variance are given by

$$\langle t_m \rangle = \frac{1}{N} \sum_{k=0}^{N-1} t_{m+k},$$

$$\langle t_m t'_m \rangle = \frac{1}{N} \sum_{k=0}^{N-1} t_{m+k} t'_{m+k}, \text{ and}$$

$$\sigma_m^2 = \langle t_m^2 \rangle - \langle t_m \rangle^2,$$

respectively.

By the direct analogy of [31,32,35] we use the finite-difference Liouville's equation of motion in the event scale for describing the evolution of discrete set of events Eq. (11), (13):

$$\frac{\Delta \xi_i(n)}{\Delta n} = i \widehat{L}(n, 1) \xi_i(n). \quad (45)$$

Here $\xi_i(n+1) = U(n+1, n) \xi_i(n)$, $U(n+1, n)$ is the "event" evolution operator. It determines the shift in linear event scale to one step Δn . The evolution operator $U(n+1, n)$ and Liouville's quasioperator $\widehat{L}(n, 1)$ can be made explicit by writing: $\widehat{L}(n, 1) = (i\Delta n)^{-1} (U(n+1, n) - 1)$.

Let's represent the set of values of the dynamical variable $\delta \xi_j = \delta \xi(j\Delta n)$, $j = 1, \dots, N$ as the k -component vector of system state in linear Euclidean space:

a) the vector of initial state of studied complex system:

$$\mathbf{A}_k^1 = \{\delta \xi_1, \delta \xi_2, \delta \xi_3, \dots, \delta \xi_k\}, \quad (46)$$

b) the vector of final system's state, which is shifted on the m events along the event scale:

$$\mathbf{A}_{m+k}^m = \{\delta \xi_{m+1}, \delta \xi_{m+2}, \delta \xi_{m+3}, \dots, \delta \xi_{m+k}\}, \quad (47)$$

where $1 \leq k \leq N$. The vectors of initial and final states, which are submitted in a similar way, are very convenient for analyzing the dynamics of the observed discrete stochastic processes with the help of discrete non-Markov processes.

To represent the ECF in a more compact form, we use the expression for the scalar product of vectors $\langle \mathbf{A}_k^1 \cdot \mathbf{A}_{m+k}^m \rangle = \sum_{j=1}^k A_j^1 A_{m+j}^m$, and the Eqs. (64) and (65):

$$a(n) = \frac{\langle \mathbf{A}_k^1(1) \mathbf{A}_{m+k}^m(n) \rangle}{\langle |\mathbf{A}_k^1(1)|^2 \rangle}. \quad (48)$$

Construction of Chain of Finite-Difference Non-Markov Kinetic Equations for the Events Correlation

Let us consider the finite-difference Liouville's equation (Eq. (44)) for the vector of final system states:

$$\frac{\Delta \mathbf{A}_{m+k}^m(n)}{\Delta n} = i \widehat{L}(n, 1) \mathbf{A}_{m+k}^m(n). \quad (49)$$

We introduce the projection operator Π , which projects the final vector $\mathbf{A}_{m+k}^m(n)$ on the direction of initial vector, and also the orthogonal operator P . The operators Π and P possess the following properties: $\Pi = |\mathbf{A}_k^1(1)\rangle \langle \mathbf{A}_k^1(1)| / \langle |\mathbf{A}_k^1(1)|^2 \rangle$, $\Pi^2 = \Pi$, $P = 1 - \Pi$, $P^2 = P$,

$\Pi P = P \Pi = 0$. They are idempotent and mutually complementary.

The initial ECF $a(n)$ (Eq. (48)) can be derived by means of projecting the vector of final states $\mathbf{A}_{m+k}^m(n)$ on the vector of initial state $\mathbf{A}_k^1(1)$:

$$\Pi \mathbf{A}_{m+k}^m(n) = \frac{\mathbf{A}_k^1(1) \langle \mathbf{A}_k^1(1) \mathbf{A}_{m+k}^m(n) \rangle}{\langle |\mathbf{A}_k^1(1)|^2 \rangle} = \mathbf{A}_k^1(1) a(n). \quad (50)$$

The operators Π and P split Euclidean vector space $A(k)$ into two mutually orthogonal subspaces:

$$\begin{aligned} A(k) &= A'(k) + A''(k), & A'(k) &= \Pi A(k), \\ A''(k) &= P A(k), & \mathbf{A}_{m+k}^m &\in A(k). \end{aligned} \quad (51)$$

As a result the finite-difference Liouville's Eq. (67) can be represented as a system of 2 equations into mutually orthogonal linear subspaces:

$$\frac{\Delta A'(n)}{\Delta n} = i \widehat{L}_{11} A'(n) + i \widehat{L}_{12} A''(n), \quad (52)$$

$$\frac{\Delta A''(n)}{\Delta n} = i \widehat{L}_{21} A'(n) + i \widehat{L}_{22} A''(n). \quad (53)$$

Here $\widehat{L}_{ij} = \Pi_i \widehat{L} \Pi_j$ are the matrix elements of Liouville's quasioperator:

$$\begin{aligned} \widehat{L} &= \widehat{L}_{11} + \widehat{L}_{12} + \widehat{L}_{21} + \widehat{L}_{22}, \\ \widehat{L}_{11} &= \Pi \widehat{L} \Pi, & \widehat{L}_{12} &= \Pi \widehat{L} P, \\ \widehat{L}_{21} &= P \widehat{L} \Pi, & \widehat{L}_{22} &= P \widehat{L} P. \end{aligned} \quad (54)$$

To solve the system of Eqs. (52), (53) we eliminate the non-reducible part, which contains $A''(n)$ and derive the self-contained equation for the reducible part $A'(n)$. In doing so we solve the Eq. (52) step-by-step and shall substitute the obtained solution into the Eq. (53). As a result we arrive at the closed kinetic equation:

$$\begin{aligned} \frac{\Delta A'(n+m\Delta n)}{\Delta n} &= i \widehat{L}_{11} A'(n+m\Delta n) \\ &+ i \widehat{L}_{12} \{1 + i\Delta n \widehat{L}_{22}\}^m A''(n) \\ &- \widehat{L}_{12} \sum_{j=1}^m \{1 + i\Delta n \widehat{L}_{22}\}^j \Delta n \\ &\times \widehat{L}_{21} A'(n + [m-j]\Delta n). \end{aligned} \quad (55)$$

TS6 Please specify which equation(s) are meant here.

588 By use of projection operators Π and P we found the
 589 closed finite-difference kinetic equation of non-Markov
 590 type for the initial ECF:

$$\frac{\Delta a(n)}{\Delta n} = i\lambda_1 a(n) - \Delta n \Lambda_1 \sum_{j=1}^m M_1(j\Delta n) a(n-j\Delta n). \quad (56)$$

592 As $\Delta n = 1$, solution of the last equation must be fol-
 593 lowing:

$$594 \quad a(n+1) = \{i\lambda_1 + 1\} a(n) - \Lambda_1 \sum_{j=1}^m M_1(j) a(n-j). \quad (57)$$

595 Here λ_1 is the proper value of Liouville's quasiopera-
 596 tor \widehat{L} , Λ_1 is the relaxation parameter, which dimension is
 597 square of frequency, $M_1(j\Delta n)$ is the normalized memory
 598 function of the first order:

$$\lambda_1 = \frac{\langle A_k^1(1) \widehat{L} A_k^1(1) \rangle}{\langle |A_k^1(1)|^2 \rangle},$$

$$599 \quad \Lambda_1 = \frac{\langle A_k^1 \widehat{L}_{12} \widehat{L}_{21} A_k^1(1) \rangle}{\langle |A_k^1(1)|^2 \rangle},$$

$$M_1(j\Delta n) = \frac{\langle A_k^1(1) \widehat{L}_{12} (1 + i\Delta n \widehat{L}_{22})^j \widehat{L}_{21} A_k^1(1) \rangle}{\langle A_k^1(1) \widehat{L}_{12} \widehat{L}_{21} A_k^1(1) \rangle}.$$

600 To obtain the finite-difference kinetic equation for the
 601 normalized event memory function of first order and, fur-
 602 ther, for the higher $(s-1)$ th orders as well, we have to re-
 603 peat the foregoing procedure step-by-step. However, we
 604 shall make use of the Gram-Schmidt orthogonalization
 605 procedure [16]:

$$606 \quad \langle \mathbf{W}_s \mathbf{W}_p \rangle = \delta_{sp} \langle |\mathbf{W}_s|^2 \rangle. \quad (58)$$

607 Where δ_{sp} is a Kronecker's symbol. Now we shall de-
 608 rive the recurrence formula $\mathbf{W}_s = \mathbf{W}_s(n)$ for defining the
 609 set of the orthogonal dynamic variables:

$$610 \quad \begin{aligned} \mathbf{W}_0 &= A_k^1, \\ \mathbf{W}_1 &= \{i\widehat{L} - \lambda_1\} \mathbf{W}_0, \\ \mathbf{W}_2 &= \{i\widehat{L} - \lambda_2\} \mathbf{W}_1 - \Lambda_1 \mathbf{W}_0, \dots \end{aligned} \quad (59)$$

611 According to the foregoing formulas we can introduce
 612 the succession of projection operators $\Pi_s = \Pi_1^{(s)}$ and the
 613 set of mutually complementary projectors $P_s = 1 - \Pi_s$,
 614 which possess the following properties:

$$615 \quad \begin{aligned} \Pi_s &= \frac{|\mathbf{W}_s\rangle\langle\mathbf{W}_s|}{\langle |\mathbf{W}_s|^2 \rangle}, & \Pi_s^2 &= \Pi_s, \\ P_s^2 &= P_s, & \Pi_s P_s &= P_s \Pi_s = 0, \\ \Pi_s P_p &= \delta_{sp} \Pi_s, & P_s P_p &= \delta_{sp} P_s. \end{aligned}$$

Each of these operators pairs Π_s, P_s splits the corre-
 sponding Euclidean vector space \mathbf{W}_s into the two mutual
 complementary subspaces: $W_s = W'_s + W''_s$, $W'_s = \Pi_s W_s$,
 $W''_s = P_s W_s$. Using the projection operator technique for
 the next orthogonal variables \mathbf{W}_s , we shall obtain the chain
 of interconnected kinetic finite-difference equations of the
 non-Markov type for the normalized correlation functions
 of the $(s-1)$ th order:

$$\frac{\Delta M_1(n)}{\Delta n} = i\lambda_2 M_1(n) - \Lambda_2 \sum_{j=1}^m M_2(j) M_1(n-j),$$

$$\dots,$$

$$\frac{\Delta M_{s-1}(n)}{\Delta n} = i\lambda_s M_{s-1}(n) - \Lambda_s \sum_{j=1}^m M_{s-1}(j) M_s(n-j). \quad (60)$$

In these equations the normalized events memory func-
 tion of the first order: $M_1(n) = \langle \mathbf{W}_1(1 + i\Delta n \widehat{L})^m \mathbf{W}_1 \rangle / \langle |\mathbf{W}_1|^2 \rangle$,
 memory function of the $(s-1)$ th order: $M_{s-1}(n) = \langle \mathbf{W}_{s-1}(1 + i\Delta n \widehat{L})^m \mathbf{W}_{s-1} \rangle / \langle |\mathbf{W}_{s-1}|^2 \rangle$,
 the proper value of the Liouville's quasioperator \widehat{L} : $\lambda_s = \langle \mathbf{W}_s \widehat{L} \mathbf{W}_s \rangle / \langle |\mathbf{W}_s|^2 \rangle$
 and the relaxation parameter $\Lambda_s = \langle |\mathbf{W}_s|^2 \rangle / \langle |\mathbf{W}_{s-1}|^2 \rangle$ are
 introduced.

The foregoing finite-difference kinetic Eqs. (60) pre-
 sent the generalization of the statistical theory [31,32,35]
 for the case of event correlations in discrete stochastic evo-
 lution of non-Hamilton complex systems.

Information Measures of Memory in Complex Systems

As an information measures of memory it is useful to ap-
 ply different dimensionless quantifiers. As a first measure
 we use the frequency dependence of non-Markovity pa-
 rameter. This measure was introduced in [31] and it is de-
 fined as:

$$643 \quad \varepsilon_i(v) = \left\{ \frac{\mu_{i-1}(v)}{\mu_i(v)} \right\}^{1/2}. \quad (61)$$

Here, $\mu_i(v)$ denotes the frequency power spectrum
 of memory function of the i th order $M_i(n)$: $\mu_i(v) = |\Delta n \sum_{n=1}^N M_i(n) \cos(2\pi n v)|^2$. The non-Markovity pa-
 rameter $\varepsilon_i(v)$ along with the memory functions enables
 us to characterize quantitatively the statistical memory ef-
 fects in discrete complex systems of various nature. Be-
 cause the functions $\mu_i(v)$ exist for each of the i th levels
 of relaxation, we obtain the statistical spectrum of param-
 eters: $\varepsilon_i(v)$, $i = 1, 2, 3, \dots$

Alternatively, a study of ‘memory’ in physiological time series for electroencephalographic (EEG) and magnetoencephalographic (MEG) signals, both of healthy subjects and patients (including epilepsy patients) has been based on the detrended-fluctuation analysis (DFA) [39,40].

The characterization of memory *per se* is based on a set of dimensionless statistical quantifiers which are capable for measuring the memory strength which is inherent to the complex dynamics.

According to [41] a second set an information memory measure can be constructed as follows:

$$\delta_i(\nu) = \left| \frac{\tilde{M}'_i(\nu)}{\tilde{M}'_{i+1}(\nu)} \right|.$$

Here, $\mu_i(\nu) = |\tilde{M}_i(\nu)|^2$ denotes the power spectrum of the corresponding memory function $M_i(t)$, $\tilde{M}'_i(\nu) = d\tilde{M}_i(\nu)/d\nu$ and $\tilde{M}_i(\nu)$ is the Fourier transform of the memory function $M_i(t)$. The measures $\varepsilon_i(\nu)$ are suitable for the quantification of the memory effects on a relative scale whereas the second set $\delta_i(\nu)$ proves to be useful for quantifying the amplification of relative memory effects occurring on different complexity levels. Both measures provide statistical criteria for comparison between the relaxation time scales and memory time scales of the process under consideration. For values obeying $\{\varepsilon, \delta\} \gg 1$ one can observe a complex dynamics characterized by the short-ranged temporal memory scales. In the memoryless limit these processes assume a δ -like memory with parameters $\varepsilon, \delta \rightarrow \infty$. When $\{\varepsilon, \delta\} > 1$ one deals with a situation with moderate memory strength, and the case where both $\varepsilon, \delta \sim 1$ typically constitutes a more regular and robust random process exhibiting strong memory features.

Manifestation of Strong Memory in Complex Systems

A fundamental role of the strong and weak memory in the functioning of the human organism and seismic phenomena can be illustrated by the example of some situations examined next. We will consider some examples of the time series for both living and for seismic systems. It is necessary to note that a comprehensive analysis of the experimental data includes the calculation and the presentation of corresponding phase portraits in some planes of the dynamic orthogonal variables, the autocorrelation time functions, the memory time functions and their frequency power spectra, etc. However, we start out by calculating two statistical quantifiers, characterizing two in-

formational measures of memory: the parameters $\varepsilon_1(\omega)$ and $\delta_1(\omega)$.

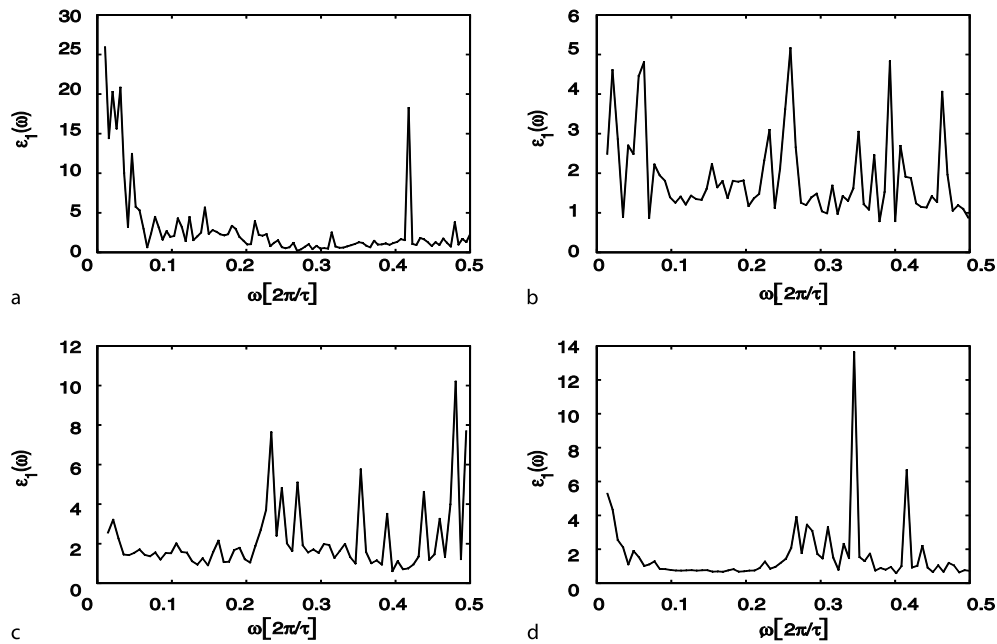
Figures 1 and 3 present the results of experimental data of pathological states of human cardiovascular systems (CVS). Figure 2 depicts the analysis for the seismic observation. Figures 4 and 5 indicate the memory effects for the patients with Parkinson disease (PD), and the last two Figs. 6, 7 demonstrate the key role of the strength of memory in the case of time series of patients suffering from photosensitive epilepsy which are contrasted with signals taken from healthy subjects. All these cases convincingly display the crucial role of the statistical memory in the functioning of complex (living and seismic) systems.

A characteristic role of the statistical memory can be detected from Fig. 1 for the typical representatives taken from patients from four different CVS-groups: (a) for healthy subject, (b) for a patient with rhythm driver migration, (c) for a patient after myocardial infarction (MI), (d) for a patient after MI with subsequent sudden cardiac death (SSCD). All these data were obtained from the short time series of the dynamics of RR-intervals from the electric signals of the human ECG's. It can be seen here that significant memory effects typically lead to the long-time correlations in the complex systems. For healthy we observe weak memory effects while and large values of the measure memory $\varepsilon_1(\omega = 0) \approx 25$. The strong memory and the long memory time (approximately, 10 times more) are being observed with the help of 3 patient groups: with RDM (rhythm driver migration) (b), after MI (c) and after MI with SSCD (d).

Figure 2 depicts the strong memory effects presented in seismic phenomena. By a transition from the steady state of Earth ((a), (b) and (c)) to the state of strong earthquake (EQ) ((d), (e), and (f)) a remarkable amplification of memory effects is highly visible. The term amplification refers to the appearance of strong memory and the prolongation of the memory correlation time in the seismic system. Recent study show that discrete non-Markov stochastic processes and long-range memory effects play a crucial role in the behavior of seismic systems. An approach, permitting us to obtain an algorithm of strong EQ forecasting and to differentiate technogenic explosions from weak EQs, can be developed thereupon.

Figure 3 demonstrates an intensification of memory effects of one order at the transition from healthy people ((a), (b) and (c)) to patient suffering from myocardial infarction. The figures were calculated from the long time series of the RR-intervals dynamics from the human ECG's. The zero frequency values $\varepsilon_1(\omega = 0)$ at $\omega = 0$ sharply reduced, approximately of the size of one order for patient as compared to healthy subjects.

TS7 Do you mean “e” here?



Correlations in Complex Systems, Figure 1

Frequency spectrum of the first information measure of memory (first point in the statistical spectrum on non-Markovity parameter) $\varepsilon_1(\omega)$ for the fourth cardiac patient groups from the short time series of RR-intervals: healthy subject (a), patient with rhythm driver migration (RDM) (b), patient after myocardial infarction (MI) (c), and patient after MI with subsequent sudden cardiac death (SCD) (d). The frequency is marked in terms of units of τ^{-1} . All spectra reveal the miscellaneous faces of statistical memory's strength. For the healthy subject one can see Markov effects and weak memory. For other three cases of cardiac diseases we note the diverse displays of strong memory. The strong memory has been accompanied by the spikes of the weak memory: for RDM on the all frequency regions, for patient with MI for the middle and high frequencies and for patient after MI with SSCD only for high frequencies. From Fig. 7 in [104]

750 Figures 4 and 5 illustrate the behavior for patients with
 751 Parkinson's disease. Figure 4 shows time recording of the
 752 pathological tremor velocity in the left index finger of
 753 a patient with Parkinson's disease (PD) for eight diverse
 754 pathological cases (with or without medication, with or
 755 without deep brain stimulation (DBS), for various DBS,
 756 medication and time conditions). Figure 5, arranged in
 757 accordance with these conditions, displays a wide variety
 758 of the memory effects in the treatment of PD's patients.
 759 Due to the large impact of memory effects this observa-
 760 tion permits us to develop an algorithm of exact diagnosis
 761 of Parkinson's disease and a calculation of the quantita-
 762 tive parameter of the quality of treatment. A physical role
 763 of the strong and long memory correlation time enables
 764 us to extract a vital information about the states of vari-
 765 ous patient on basis of notions of correlation and memory
 766 times.

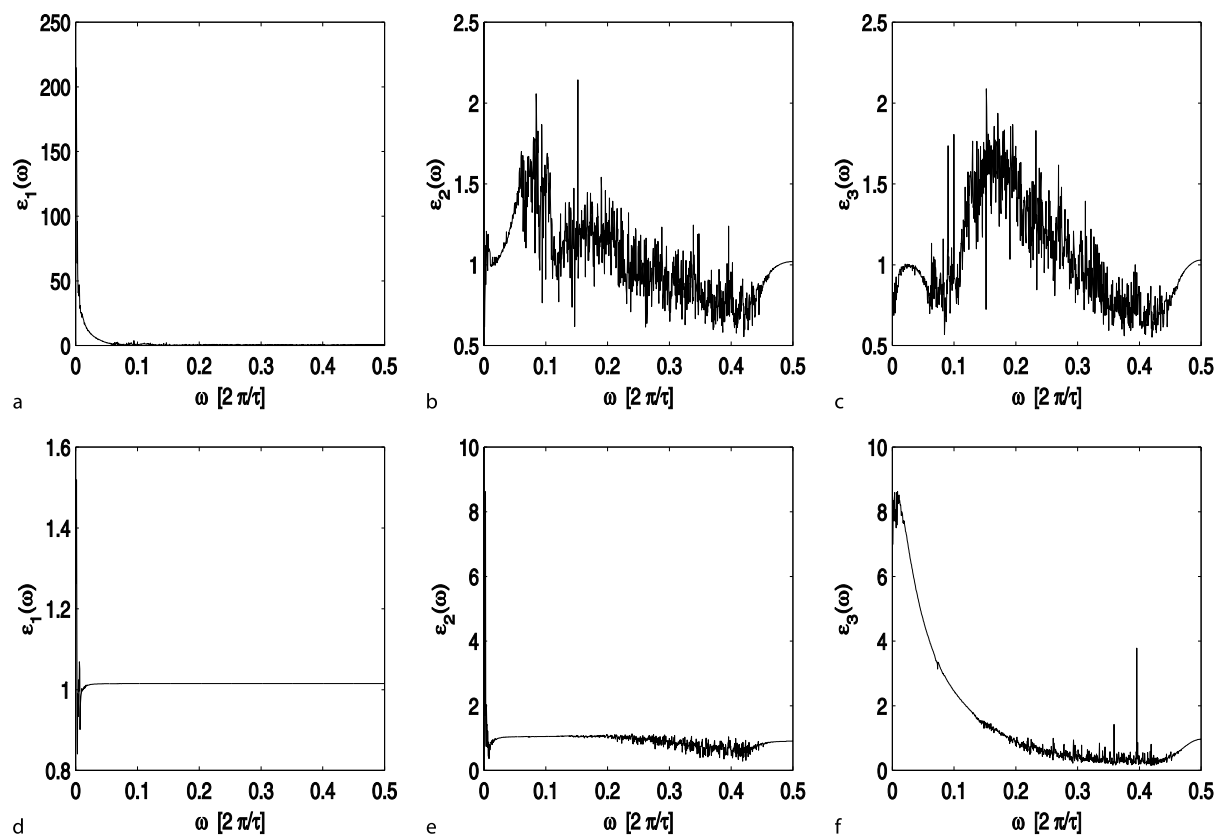
767 According to Figs. 6 and 7 specific information
 768 about the physiological mechanism of photosensitive
 769 epilepsy (PSE) was obtained from the analysis of the strong
 770 memory effects via the registration the neuromagnetic

771 responses in recording of magnetoencephalogram (MEG)
 772 of the human brain core. Figure 6 presents the topographic
 773 dependence of the first level of the second memory mea-
 774 sure $\delta_1(\omega = 0; n)$ for the healthy subjects in the whole
 775 group (upper line) vs. patients (lower line) for red/blue
 776 combination of the light stimulus. This topographic de-
 777 pendence of $\varepsilon_1(\omega = 0; n)$ depicted in Fig. 6 clearly demon-
 778 strates the existence of long-range time correlation. It is
 779 accompanied by a sharp increase of the role of the statisti-
 780 cal memory effects in the all MEG's sensors with sensor
 781 numbers $n = 1, 2, \dots, 61$ of the patient with PSE in com-
 782 parison with healthy peoples. A sizable difference between
 783 the healthy subject and a subject with PSE occurs.

784 To emphasize the role of strong memory one can contin-
 785 ue studying the topographic dependence in terms of the
 786 novel informational measure, the index of memory, de-
 787 fined as:

$$v(n) = \frac{\delta_1^{\text{healthy}}(0; n)}{\delta_1^{\text{patient}}(0; n)}, \quad (62)$$

788 see in Fig. 7.
 789



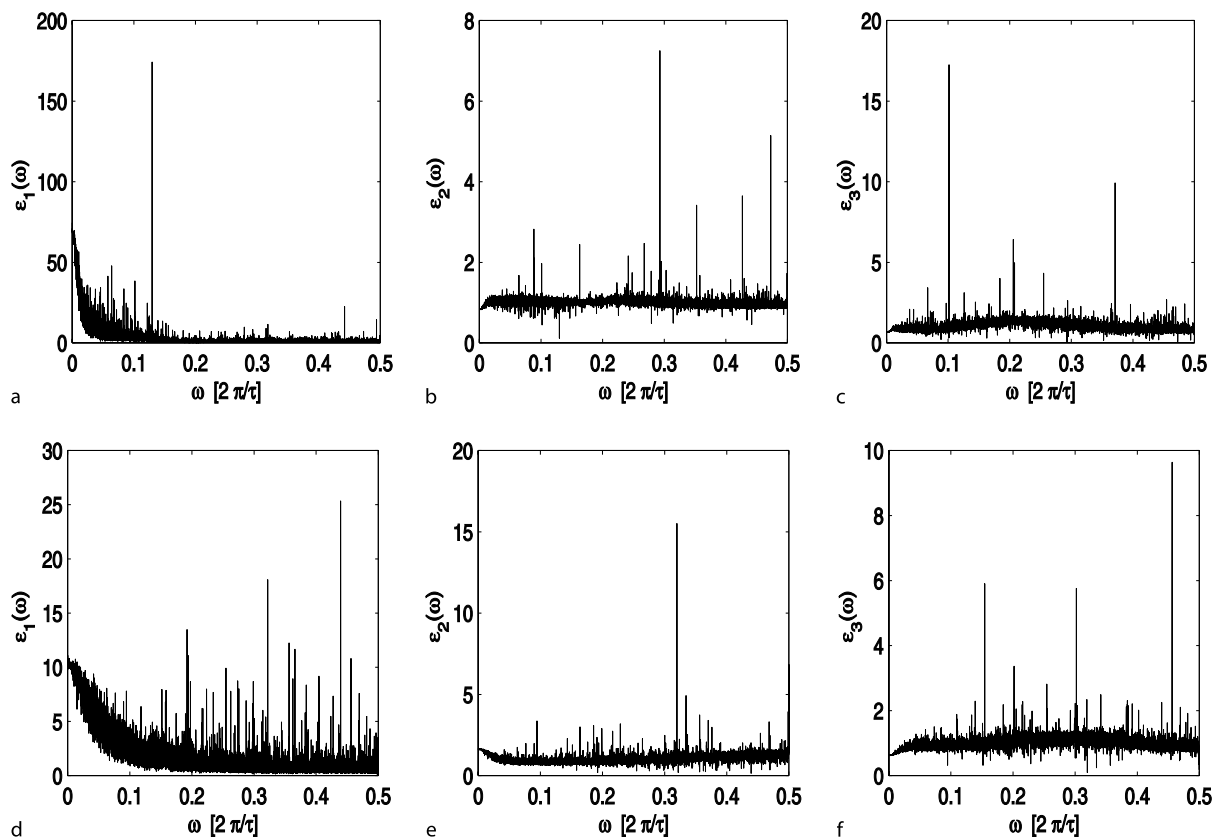
Correlations in Complex Systems, Figure 2

Frequency spectra of the first three points of the first measure of memory (non-Markovity parameters) $\varepsilon_1(\omega)$, $\varepsilon_2(\omega)$, and $\varepsilon_3(\omega)$ for the seismic phenomena: a, b, c long before the strong Earthquake (EQ) for the steady state of Earth and d, e, f during the strong EQ. Markov and quasi-Markov behavior of seismic signals with manifestation of the weak memory is observed only for ε_1 in state before the strong EQ. All remaining cases b, c, d and e, f relate to non-Markov processes. Strong non-Markovity and strong memory is typical for case d (state during the strong EQ). In behavior of $\varepsilon_2(\omega)$ and $\varepsilon_3(\omega)$ one can see a transition from quasi-Markovity (at low frequencies) to strong non-Markovity (at high frequencies). From Fig. 6 in [105]

790 This measure quantifies the detailed memory effects
791 in the individual MEG sensors of the patient with PSE
792 versus the healthy group. A sharp increase of the role
793 of the memory effects in the stochastic behavior of the
794 magnetic signals is clearly detected in sensor numbers
795 $n = 10, 46, 51, 53$ and 59 . The observed points of MEG
796 sensors locate the regions of a protective mechanism
797 against PSE in a human organism: frontal (sensor 10),
798 occipital (sensors 46, 51 and 53) and right parietal (sen-
799 sor 59) regions. The early activity in these sensors may re-
800 flect a protective mechanism suppressing the cortical hy-
801 peractivity due to the chromatic flickering.

802 We remark that some early steps towards understand-
803 ing the normal and various catastrophic states of com-
804 plex systems have already been taken in many fields of
805 science such as cardiology, physiology, medicine, neuro-
806 logy, clinical neurophysiology, neuroscience, seismology

and so forth. With the underlying systems showing frac- 807
tural and complicated spatial structures numerous studies 808
applying the linear and nonlinear time series analysis to 809
various complex systems have been discussed by many 810
authors. Specifically the results obtained shows evidence 811
of the significant nonlinear structure evident in the reg- 812
istered signals in the control subjects, whereas nonlinear- 813
ity for the patients and catastrophic states were not de- 814
tected. Moreover the couplings between distant parts and 815
regions were found to be stronger for the control subjects. 816
These prior findings are leading to the hypothesis that the 817
real normal complex systems are mostly equipped with 818
significantly nonlinear subsystems reflecting an inherent 819
mechanism which stems against a synchronous excitation 820
vs. outside impact or inside disturbances. Such nonlinear 821
mechanisms are likely absent in the occurrence of catas- 822
trophical or pathological states of the complex systems. 823



Correlations in Complex Systems, Figure 3

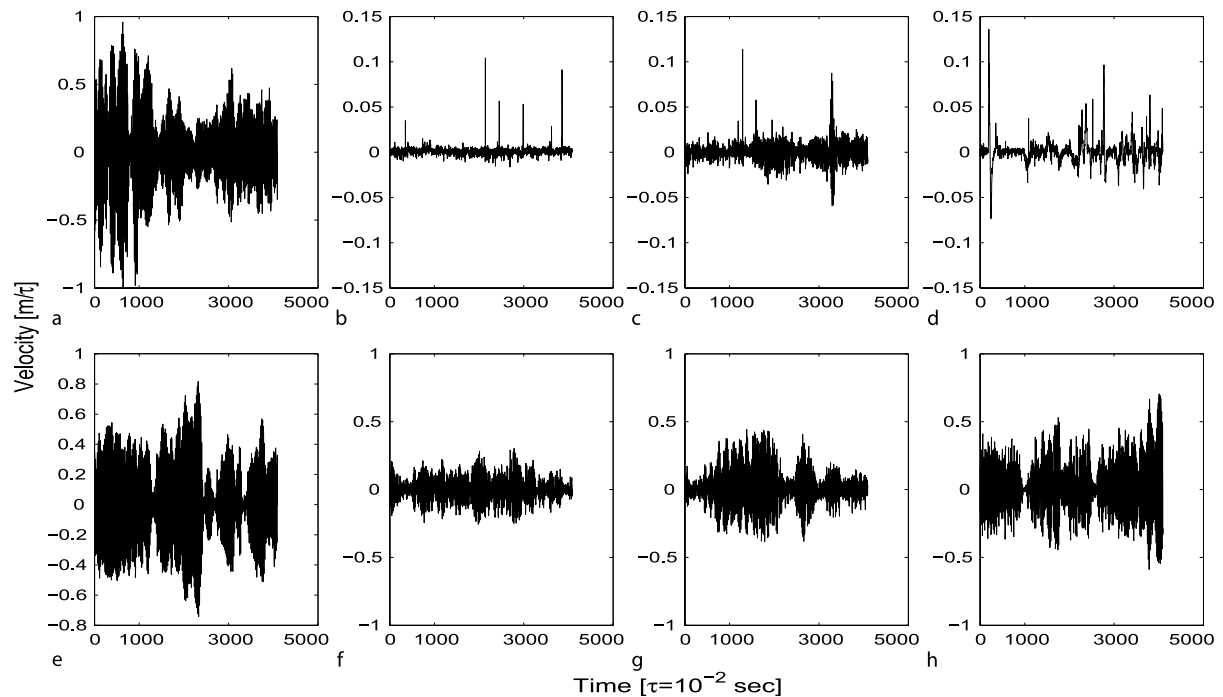
The frequency dependence of the first three points of non-Markovity parameter (NMP) for the healthy person (a), (b), (c) and patient after myocardial infarction (MI) (d), (e), (f) from the time dynamics of RR-intervals of human ECG's for the case of the long time series. In the spectrum of the first point of NMP $\varepsilon_1(\omega)$ there is an appreciable low-frequency (long time) component, which concerns the quasi-Markov processes. Spectra NMP $\varepsilon_2(\omega)$ and NMP $\varepsilon_3(\omega)$ fully comply with non-Markov processes within the whole range of frequencies. From Fig. 6 in [106]

824 From the physical point of view our results can be used
 825 as a toolbox for testing and identifying the presence or absence
 826 of various memory effects as they occur in complex
 827 systems. The set of our memory quantifiers is uniquely associated
 828 with the appearance of memory features in the chaotic behavior
 829 of the observed signals. The registration of the behavior belonging
 830 to these indicators, as elucidated here, is of beneficial use for
 831 detecting the catastrophic or pathological states in the complex
 832 systems. There exist alternative quantifiers of different nature
 833 as well, such as the Lyapunov's exponent, Kolmogorov-Sinai
 834 entropy, correlation dimension, etc., which are widely used in
 835 nonlinear dynamics and relevant applications. In the present
 836 context, we have found out that the employed memory
 837 measures are not only convenient for the analysis but are
 838 also ideally suitable for the identification of anomalous
 839 behavior occurring in complex systems. The search for other
 840 quantifiers, and foremost, the ways of optimization of such

842 measures when applied to the complex discrete time
 843 dynamics presents a real challenge. Especially this objective
 844 is met when attempts are made towards the identification
 845 and quantification of functioning in complex systems.
 846 This work presents initial steps towards the understanding
 847 of basic foundation of anomalous processes in complex
 848 systems on the basis of a study of the underlying memory
 849 effects and connected with this, the occurrence of long
 850 lasting correlations.

851 **Some Perspectives on the Studies of Memory** 852 **in Complex Systems**

853 Here we present a few outlooks on the fundamental role
 854 of statistical memory in complex systems. This involves
 855 the issue of studying cross-correlations. The statistical theory
 856 of stochastic dynamics of cross-correlation can be created
 857 on the basis of the mentioned formalism of projection



Correlations in Complex Systems, Figure 4

Pathological tremor velocity in the left index finger of the sixth patient with Parkinson's disease (PD). The registration of Parkinsonian tremor velocity is carried out for the following conditions: **a** "OFF-OFF" condition (no any treatment), **b** "ON-ON" condition (using deep brain stimulation (DBS) by electromagnetic stimulator and medicaments), **c** "ON-OFF" condition (DBS only), **d** "OFF-ON" condition (medicaments (L-Dopa) only), **e-h** the "15 OFF", "30 OFF", "45 OFF", "60 OFF" conditions – the patient's states 15 (30, 45, 60) minutes after the DBS is switched off, no treatment. Let's note the scale of the pathological tremor amplitude (see the vertical scale). Such representation of the time series allows us to note the increase or the decrease of pathological tremor. From Fig. 1 in [107]

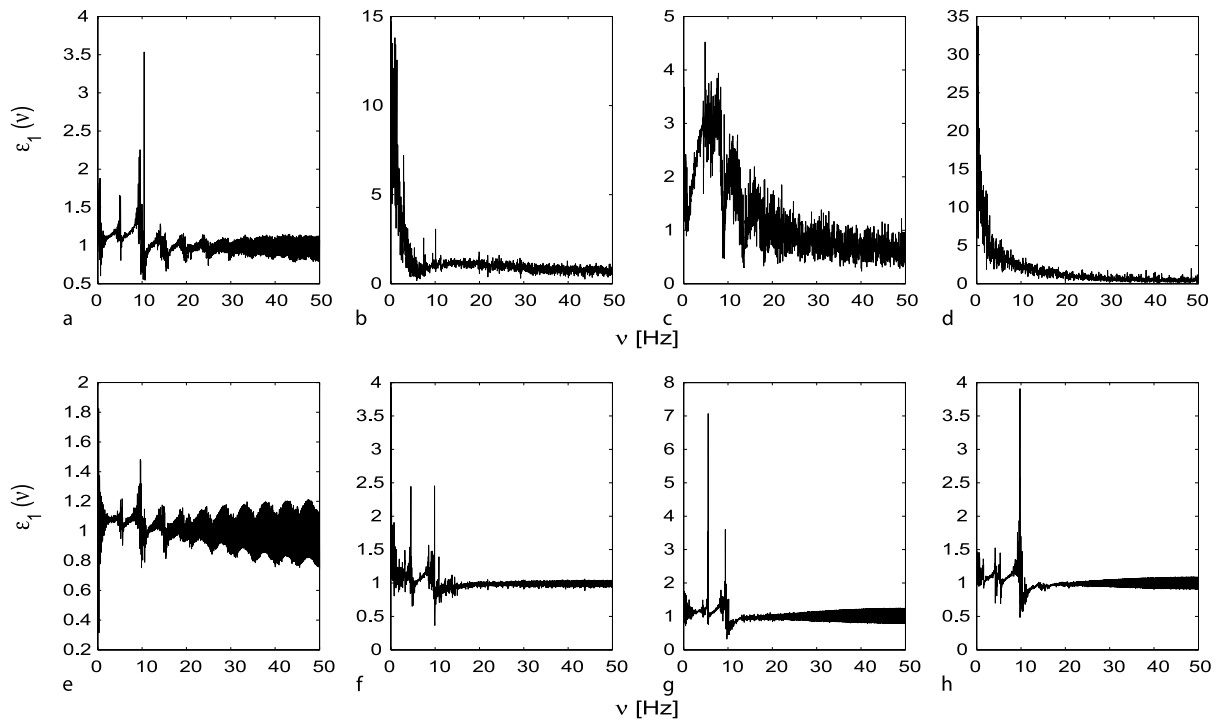
858 operators technique in the linear space of random vari- 879
 859 ables. As a result we obtain the cross-correlation memory 880
 860 functions (MF's) revealing the statistical memory effects in 881
 861 complex systems. Some memory quantifiers will appear sim- 882
 862 ultaneously which will reflect cross-correlation between 883
 863 different parts of CS. Cross-correlation MF's can be very 884
 864 useful for the analysis of the weak and strong interactions, 885
 865 signifying interrelations between the different groups of 886
 866 random variables in CS. Besides that the cross-correlation 887
 867 can be important for the problem of phase synchroniza- 888
 868 tion, which can find a unique way of studying of synchro- 889
 869 nization phenomena in CS that has a special importance 890
 870 when studying aspects of brain and living systems dynam- 891
 871 ics. 892

872 Some additional information about the strong and 893
 873 weak memory effects can be extracted from the observa- 894
 874 tion of correlation in CS in the random event's scales. 895
 875 Similar effects are playing a crucial role in the differen- 896
 876 tiation between stochastic phenomena within astrophys- 897
 877 ical systems, for example, in galaxies, pulsars, quasars, mi- 898
 878 croquasars, lacertides, black holes, etc. One of the most 899

important area of application of developed approach is 879
 a bispectral and polyspectral analysis for the diverse CS. 880
 From the mathematical point of view a correct definition 881
 of the spectral properties in the functional space of ran- 882
 dom functions is quite important. A variety of MF's arises 883
 in the quantitative analysis of the fine details of memory 884
 effects in a nonlinear manner. The quantitative control of 885
 the treatment quality in the diverse areas of medicine and 886
 physiology may be one of the important biomedical appli- 887
 cation of the manifestation of the strong memory effects. 888

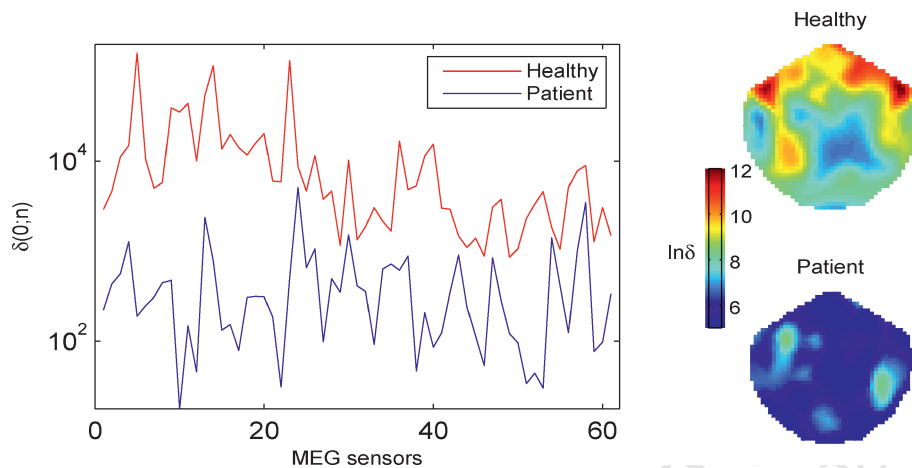
889 These and other features of memory effects in CS call 890
 for an advanced development of brain studies on the ba- 891
 sis of EEG's and MEG's data, cardiovascular, locomotor 892
 and respiratory human systems, in the development of the 893
 control system of information flows in living systems. An 894
 example is the prediction of strong EQ's and the clear dif- 895
 ferentiation between the occurrence of weak EQ's and the 896
 technogenic explosions, etc. 897

898 In conclusion, we hope that the interested reader 899
 becomes invigorated by this presentation of correlation 899
 and memory analysis of the inherent nonlinear system



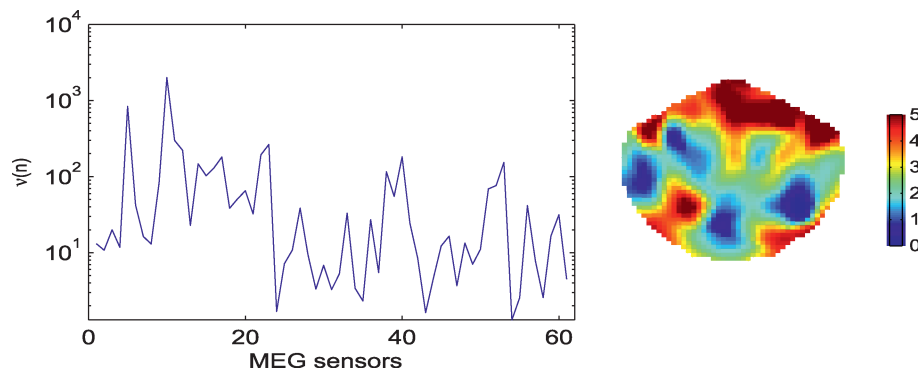
Correlations in Complex Systems, Figure 5

The frequency dependence of the first point of the non-Markovity parameter $\varepsilon_1(\nu)$ for pathological tremor velocity in the patient. As an example, the sixth patient with Parkinson's disease is chosen. The figures are submitted according to the arrangement of the initial time series. The characteristic low-frequency oscillations are observed in frequency dependence (a, e–h), which get suppressed under medical influence (b–d). The non-Markovity parameter reflects the Markov and non-Markov components of the initial time signal. The value of the parameter on zero frequency $\varepsilon_1(0)$ reflects the total dynamics of the initial time signal. The maximal values of parameter $\varepsilon_1(0)$ correspond to small amplitudes of pathological tremor velocity. The minimal values of this parameter are characteristic of significant pathological tremor velocities. The comparative analysis of frequency dependence $\varepsilon_1(\nu)$ allows us to estimate the efficiency of each method of treatment. From Fig. 5 in [107]



Correlations in Complex Systems, Figure 6

The topographic dependence of the first point of the second measure of memory $\delta_1(\omega = 0; n)$ for the healthy on average in the whole group (*upper line*) vs. patient (*lower line*) for R/B combination of the light stimulus. One can note the singular weak memory effects for the healthy on average in sensors with No. 5, 23, 14, 11 and 9



Correlations in Complex Systems, Figure 7

The topographic dependence of the memory index $v(n) = v_1(n; 0)$ for the the whole group of healthy on average vs. patient for an R/B combination of the light stimulus. Strong memory in patient vs. healthy appears clearly in sensors with No. 10, 5, 23, 40 and 53

dynamics of varying complexity. He can find further details how significant memory effects typically cause long time correlations in complex systems by inspecting more closely some of the published items in [42–103].

There are the relationships between standard fractional and polyfractal processes and long-time correlation in complex systems, which were explained in [39,40,44,45, 46,49,53,54,60,62,64,76,79,83,84,94] in detail.

Example of using the Hurst exponent over time for testing the assertion that emerging markets are becoming more efficient can be found in [51].

While over 30 measures of complexity have been proposed in the research literature one can distinguish [42,55, 66,81,89,99] with the specific designation of long-time correlation and memory effects.

Methods [48,57] are focused on long range correlation processes that are nonlocal in time and whence show memory effects.

The statistical characterization of the nonstationarities in real-world time series is an important topic in many fields of research and some numerous methods of characterizing nonstationary time series were offered in [59, 65,84].

Long-range correlated time series have been widely used in [52,61,63,68,74] for the theoretical description of diverse phenomena.

Example of the study an anatomy of extreme events in a complex adaptive system can be found in [67].

Approaches for modeling long-time and long-range correlation in complex systems from time series are investigated and applied to different examples in [50,56,69,70, 73,75,80,82,86,100,101,102].

Detecting scale invariance and its fundamental relationships with statistical structures is one of the most relevant problems among those addressed correlation analysis [47,71,72,91].

Specific long-range correlation in complex systems are the object of active research due to its implications in the technology of materials and in several fields of scientific knowledge with the use of quantified histograms [78], decrease of chaos in heart failure [85], scaling properties of ECG's signals fluctuations [87], transport properties in correlated systems [88] etc.




It is demonstrated in [43,92,93] how ubiquity of the long-range correlations is apparent in typical and exotic complex statistical systems with application to biology, medicine, economics and to time clustering properties [95,98].


The scale-dependent wavelet and spectral measures for assessing cardiac dysfunction have been used in [97].

In recent years the study of an increasing number of natural phenomena that appear to deviate from standard statistical distributions has kindled interest in alternative formulations of statistical mechanics [58,101].

At last, papers [77,90] present the samples of the deep and multiple interplay between discrete and continuous long-time correlation and memory in complex systems and the corresponding modeling the discrete time series on the basis of physical Zwanzig–Mori's kinetic equation for the Hamilton statistical systems.

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